

Soft Matter in Chemical Safety Science

13/07/2026

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Safety, Environmental
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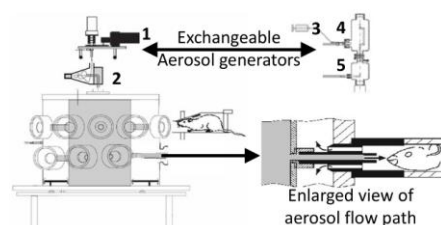
Context :

Assuring safety of consumer products

Safety without animal testing

'Traditional' Risk Assessment

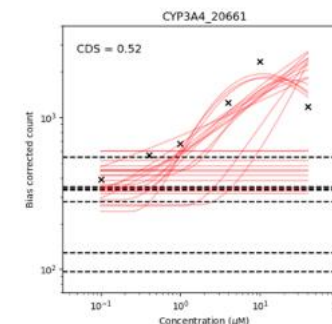
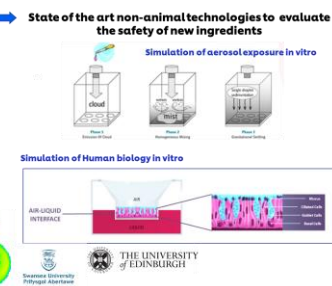
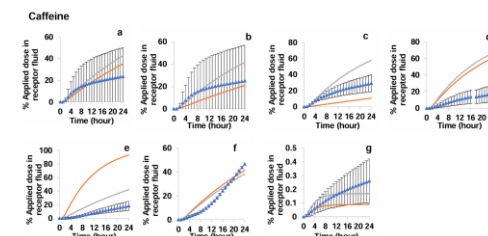
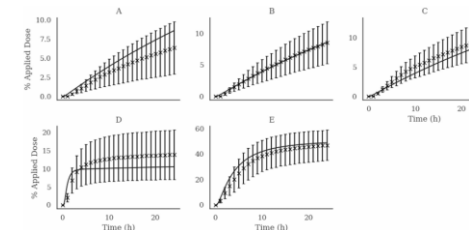
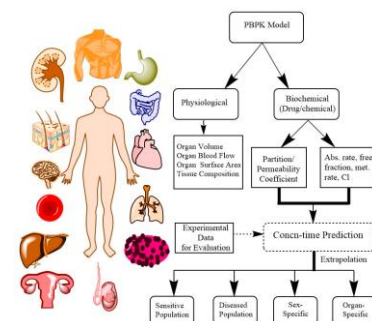
Historically animal testing was the typical method



LABORATORY TEST

'Next Generation' Risk Assessment

based on advances in human biology and in vitro/computational modelling

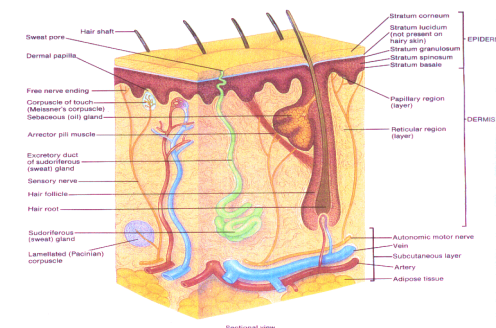
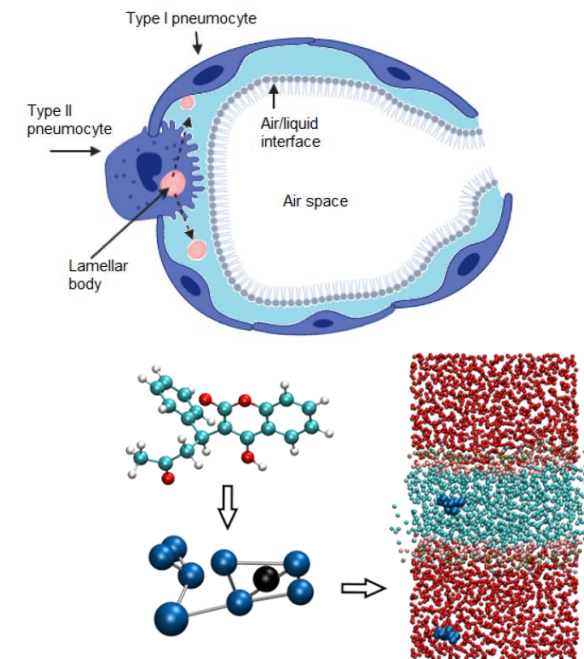


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Where does Soft Matter come in?

Today's Showcase examples:

1. Lung Surfactant Disruption -> Dilational Rheology
2. Lipid Membrane modelling -> Coarse Grained Simulation
3. Skin Penetration -> Polymers and Solution theory



Lung Surfactant Inhibition

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Surfactant

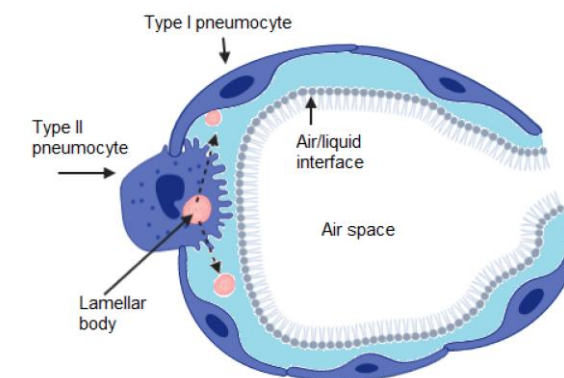
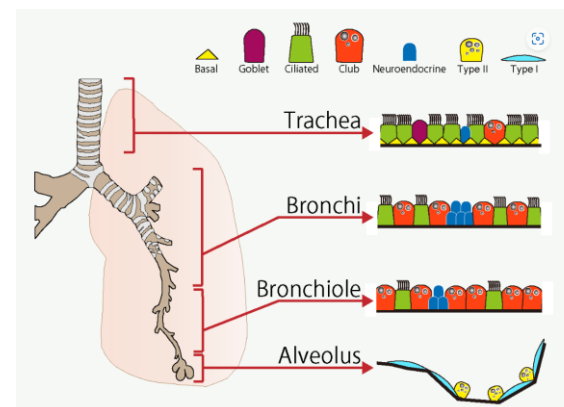
Surface Pressure $\Pi(\Gamma)$

Surface Concentration Γ

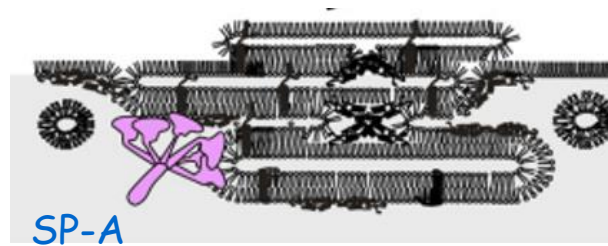
As surface expands and contracts molecules migrate between bulk and surface

Surfactant Proteins modify the process by forming subsurface structures

Increases the rate at which the surfactants re-adsorb during inhalation



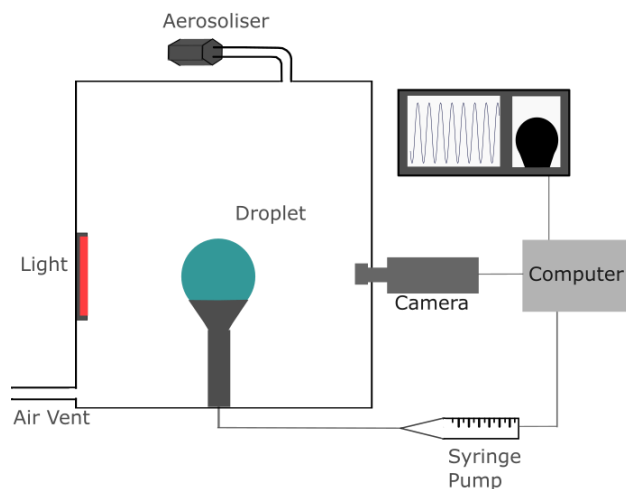
dataphysics-instruments.com



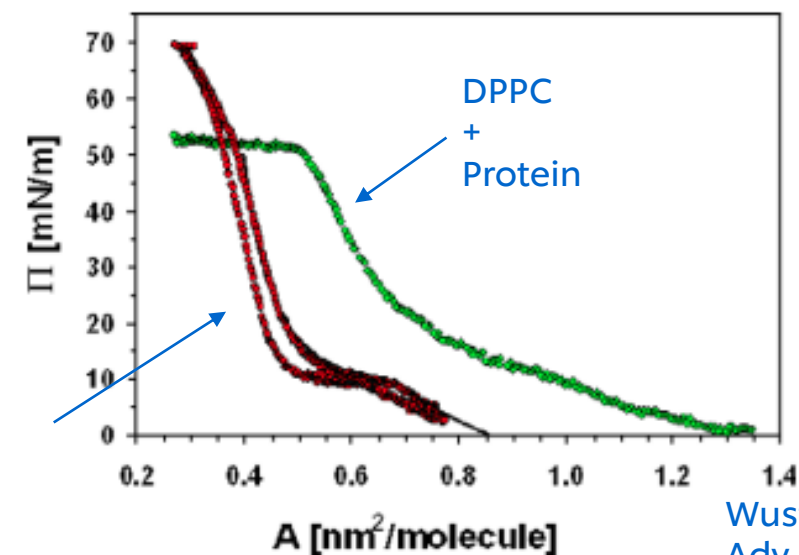
Formation of three dimensional structures increases elasticity of monolayer

Without lung surfactant to modify the elasticity of alveoli collapse during exhalation as seen in pre-term infants

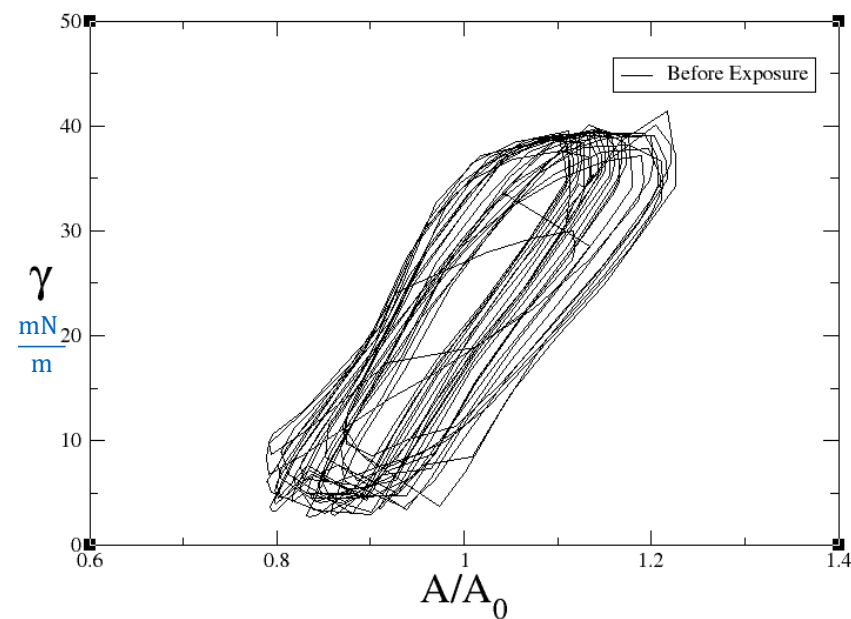
Can the disruption of breathing due to aerosolised compounds be due to modifications of the Lung surfactant rheology?



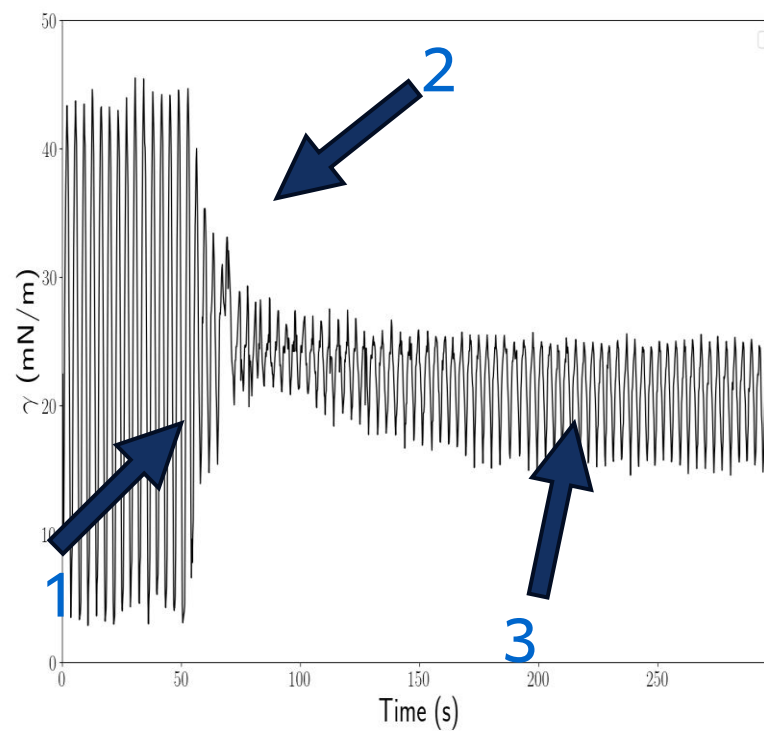
Pure DPPC



Wustneck et al.
Adv. Coll. Surf. Sci.2006

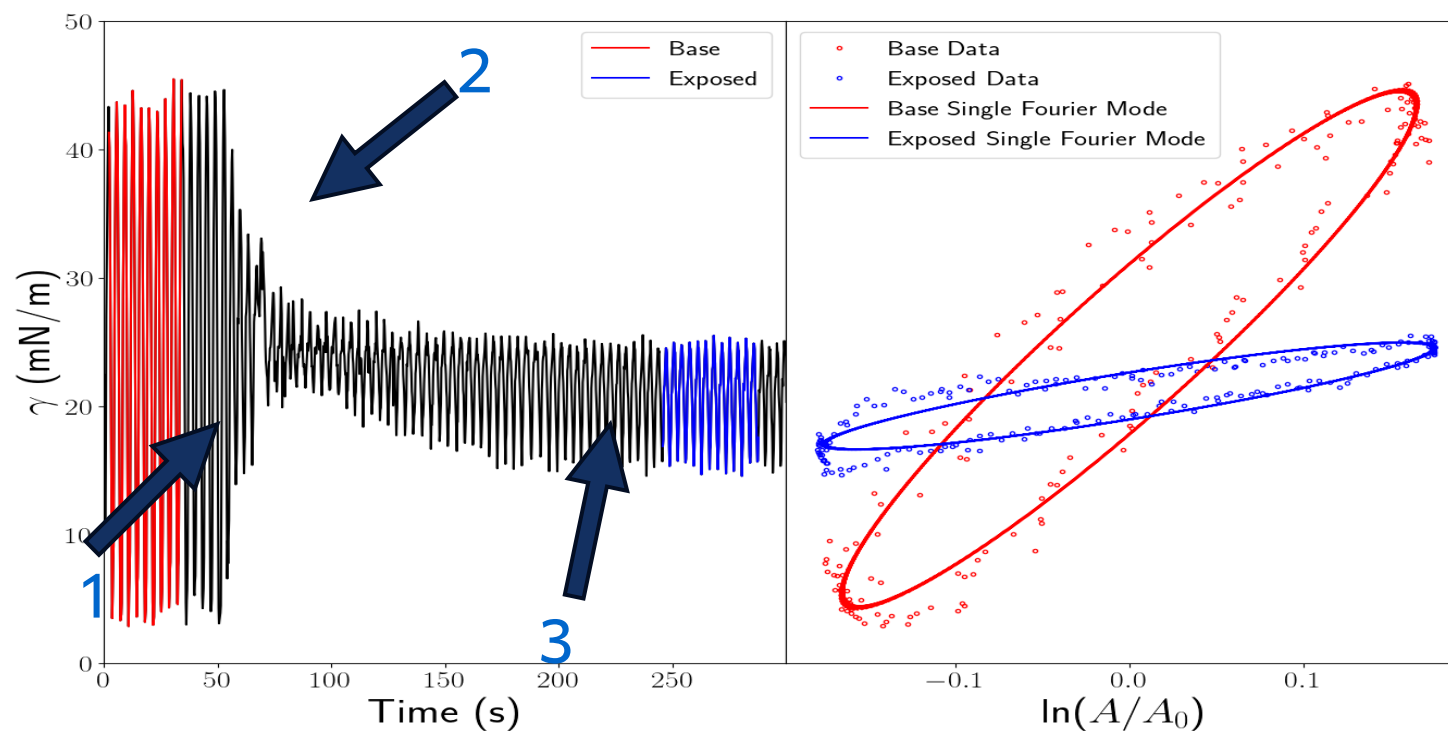


Experiments – (Alkylsiloxane Polymer)



1. Base Response established before infusion
2. Infusion begins at 40s
3. New response appears after short time

Experiments – (Alkylsiloxane Polymer)

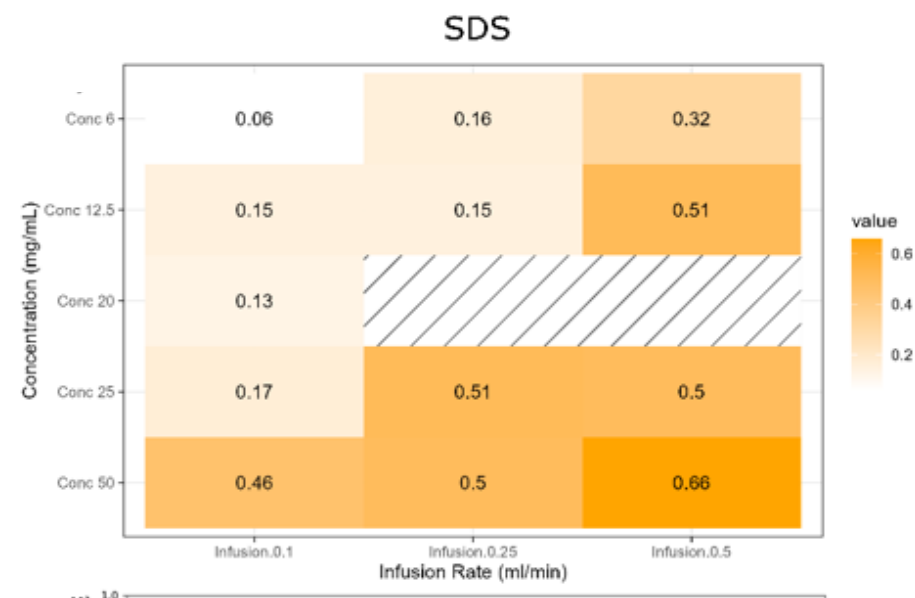


1. Base Response established before aerosol infusion
2. Infusion begins at 40s and continues
3. New **steady** response appears after short time

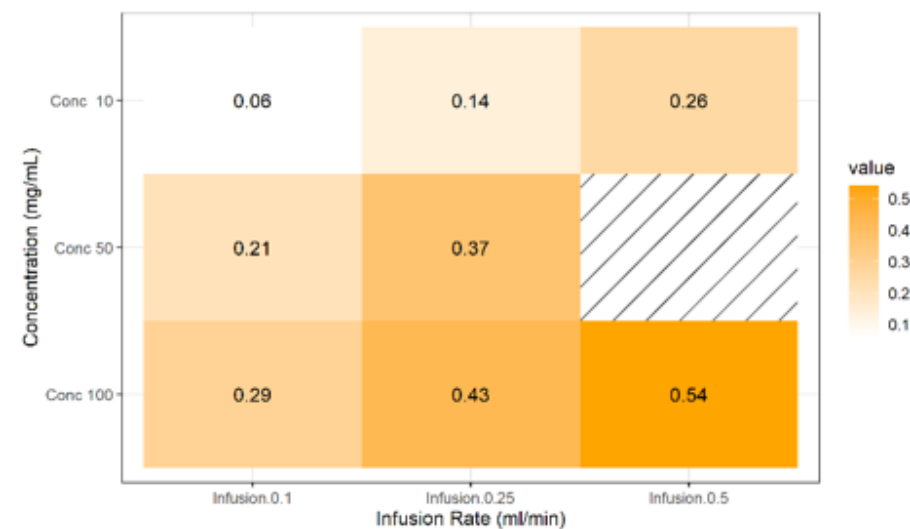
Experiments

$$|E^*| = \sqrt{E'^2 + E''^2}$$

$$\Delta \tilde{E} = \frac{|E_{post}^*| - |E_{pre}^*|}{|E_{pre}^*|}$$



Polyhexanide



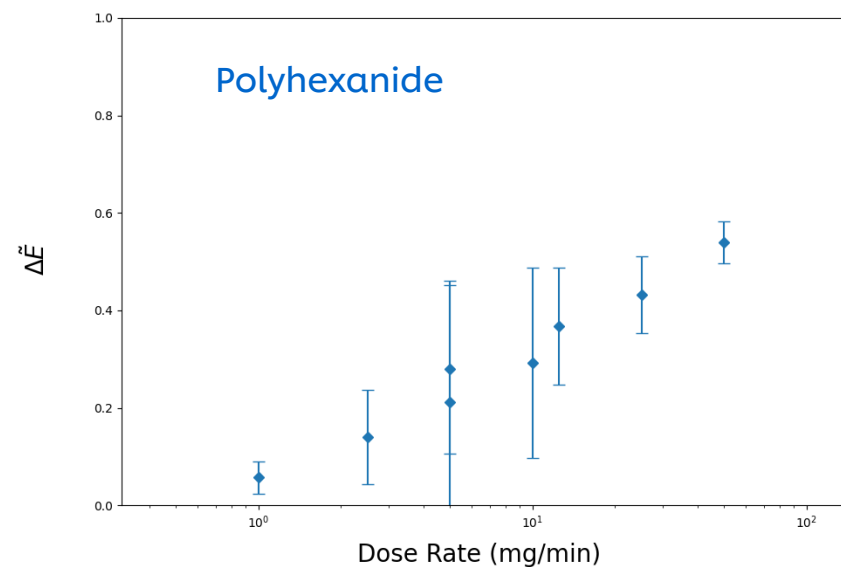
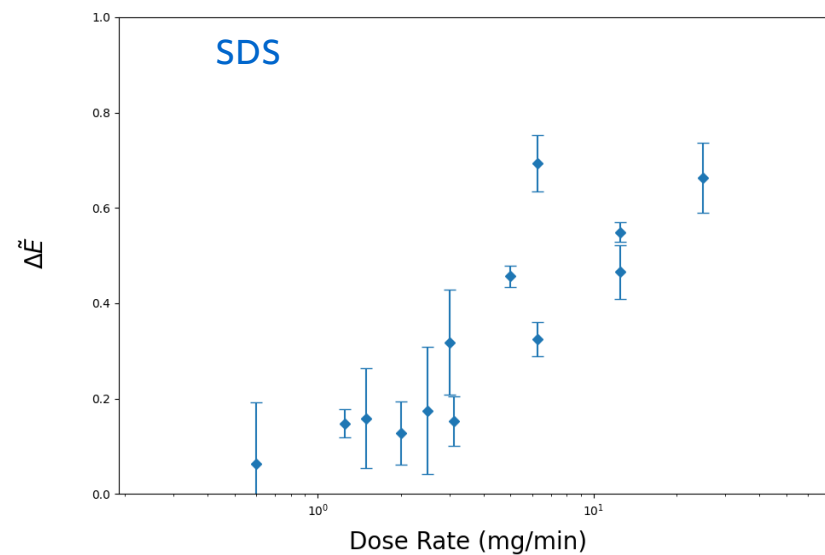
Experiments

$$|E^*| = \sqrt{E'^2 + E''^2}$$

$$\Delta \tilde{E} = \frac{|E_{post}^*| - |E_{pre}^*|}{|E_{pre}^*|}$$

$$\text{Dose Rate} = \text{Chemical Concentration} \times \text{Infusion Rate}$$

Now can we understand what's going on based on surfactant physics?



Modelling - Volmer isotherm

Assume that lung surfactant on surface behaves as a two dimensional gas with surface concentration Γ and migrates between bulk and surface continuously

Surface Tension $\gamma = \gamma_0 - k_B T \Pi(\Gamma)$ Surface Pressure $\Pi(\Gamma) = m \frac{\Gamma_\infty \Gamma}{\Gamma_\infty - \Gamma}$

Total Surfactant Flux $Q = \frac{d(\Gamma A)}{dt}$

Rate of change surfactant concentration $\frac{d\Gamma}{dt} = k_a C(\Gamma_\infty - \Gamma) - k_d \Gamma e^{\frac{\xi(\Gamma)}{k_B T}} - \frac{\Gamma}{A} \frac{dA}{dt}$

Non-local Interactions $\xi(\Gamma) = k_B T \frac{m\Gamma}{\Gamma_\infty - \Gamma}$

Rate constants k_a, k_d Empirical Scaling Parameter m

Maximum Concentration $\Gamma_\infty^{-1} = 50 \text{ \AA}^2$

Kralchevsky et al.
Handbook of Surfactant Science
2008

Model – Xenobiotic Effects

Assume that the aerosolised compound is introduced at fixed rate $\dot{\Gamma}_x$

$$\gamma = \gamma_0 - k_B T \Gamma_\infty \Pi(\Gamma, \Gamma_x)$$

Desorption rate of compound $k_{x,d}$

$$\Pi(\Gamma, \Gamma_x) = m \frac{\Gamma + \Gamma_x}{\Gamma_\infty - \Gamma - \Gamma_x} + \frac{\beta_x}{k_B T} (\Gamma_x / \Gamma_\infty)^2$$

Non-local Interaction xenobiotic parameter β_x

$$\frac{d\Gamma}{dt} = k_a C (\Gamma_\infty - \Gamma - \Gamma_x) - k_d \Gamma e^{\frac{\xi(\Gamma, \Gamma_x)}{k_B T}} - \frac{\Gamma}{A} \frac{dA}{dt}$$

$$\dot{\Gamma}_x = \alpha \times \text{Dose Rate}$$

$$\frac{d\Gamma_x}{dt} = \dot{\Gamma}_x - k_{x,d} \Gamma_x e^{\frac{\xi(\Gamma, \Gamma_x)}{k_B T}} - \frac{\Gamma_x}{A} \frac{dA}{dt}$$

These three parameters are used to fit our model for each chemical studied

$$\xi(\Gamma, \Gamma_x) = k_B T m \frac{\Gamma + \Gamma_x}{\Gamma_\infty - \Gamma - \Gamma_x} + \beta_x \Gamma_x / \Gamma_\infty$$

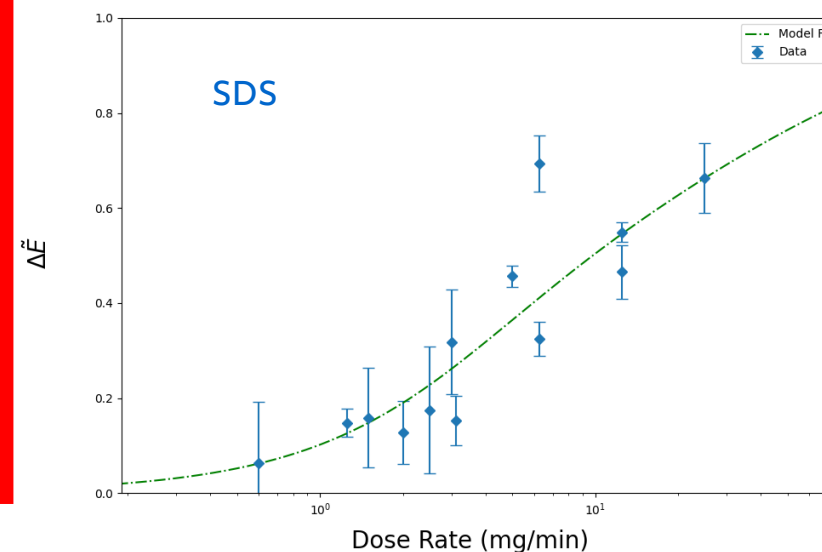
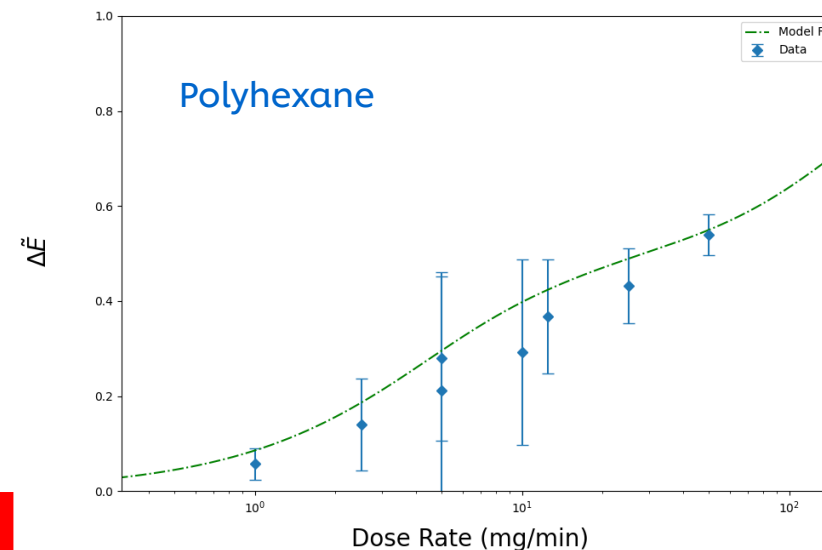
Modelling – Xenobiotic Effects

Model Accurately reproduces observed change in Lissajous curves with increasing dose rate

Model also reproduces observed change in dilational modulus for Polyhexane & SDS

Conclusions

- Inhibition of function of lung surfactant function demonstrated to be linked to compound altering dilational rheology
- In vitro study reproduces dose rate dependence/potencies seen in literature
- Modelling successfully fits all data from experiments suggesting mechanism is generic

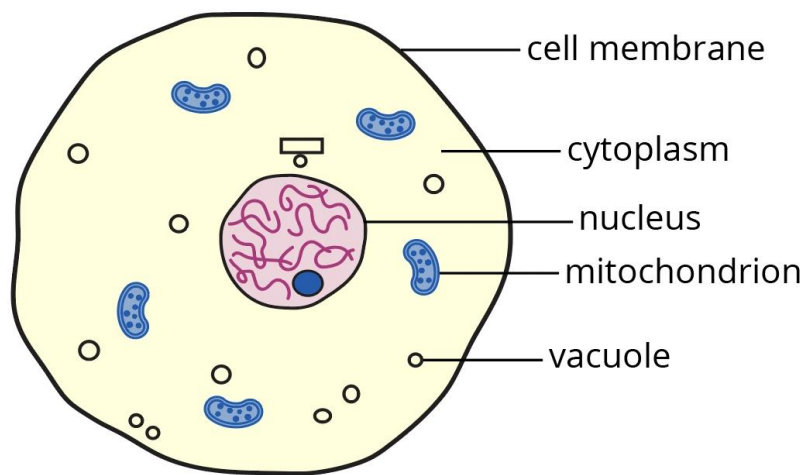


Predicting Surfactant Toxicity using Coarse Grained MD Simulations

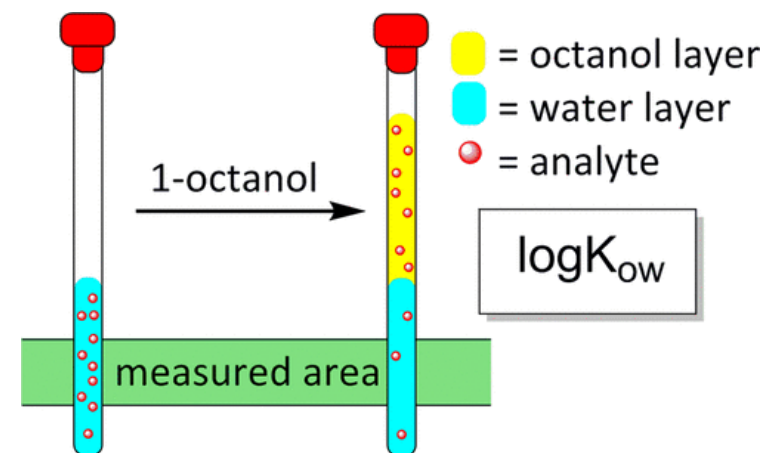


LogK_{ow} in pharmacology

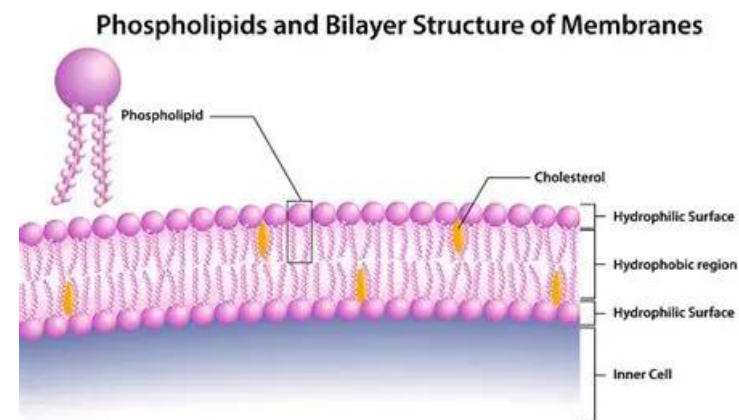
Widely used to determine the bioavailability of drugs as a measure of their lipophilicity



Lipophilicity assumed to drive bioavailability because of molecular partitioning into membranes K_{mw}



Cumming et al. *ACS omega* (2017)



K_{ow} in pharmacology

$$\log K_{mw} = 0.92(\pm 0.062) \log K_{ow} + 0.37(\pm 0.20)$$

Klamt et al. J. Phys. Chem. B 2008

$$\log K_{mw} = 1.01 \log K_{ow} + 0.12$$

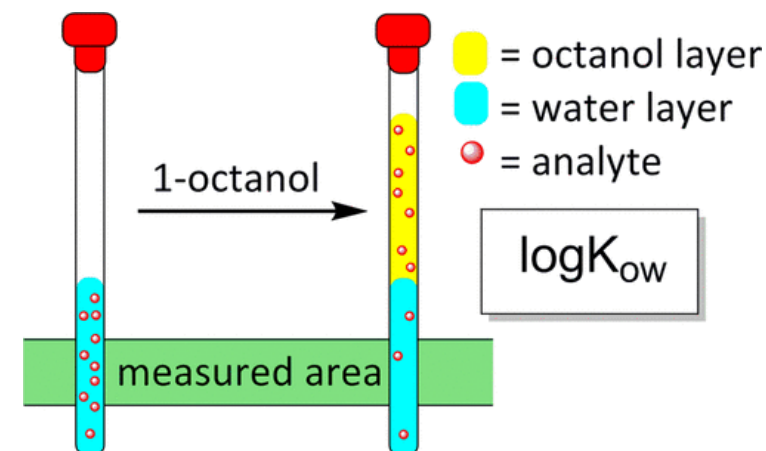
Bittermann et al., Chemosphere, 2016

Lucky coincidence that measuring K_{ow} gets you pretty close to true quantity $\log K_{mw}$

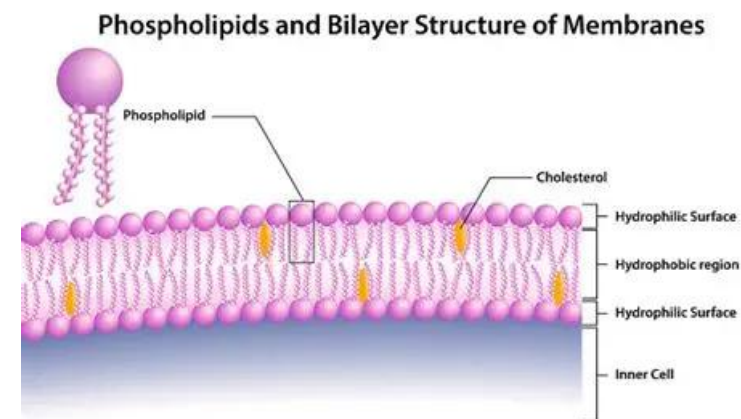
Will not work for **surfactants**, charged or large molecules

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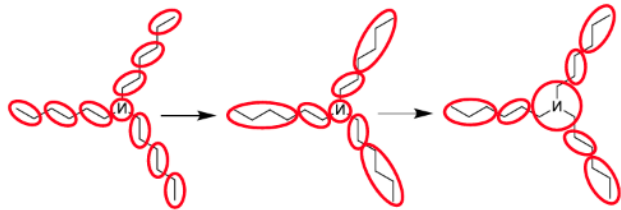
Cumming et al. *ACS omega* (2017)



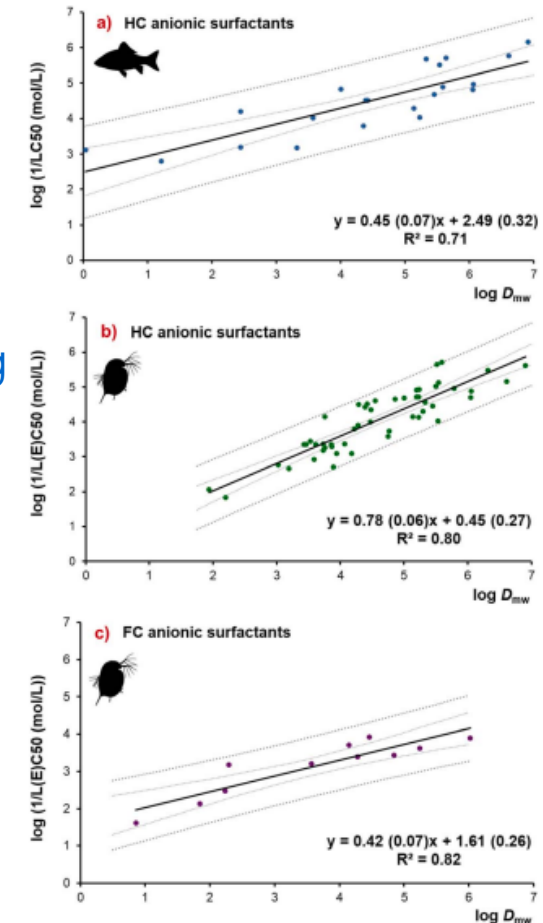
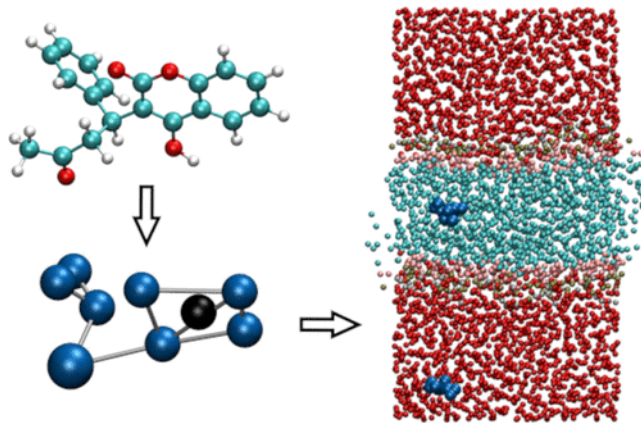
www.shutterstock.com

Environmental Toxicology being doing - Simulations

Automated Coarse grained mapping
Algorithm developed by Durham



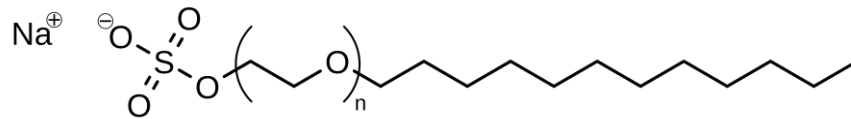
Membrane-Water Partitioning
applied successfully for
environmental impacts



Potter et al. JCTC 2021

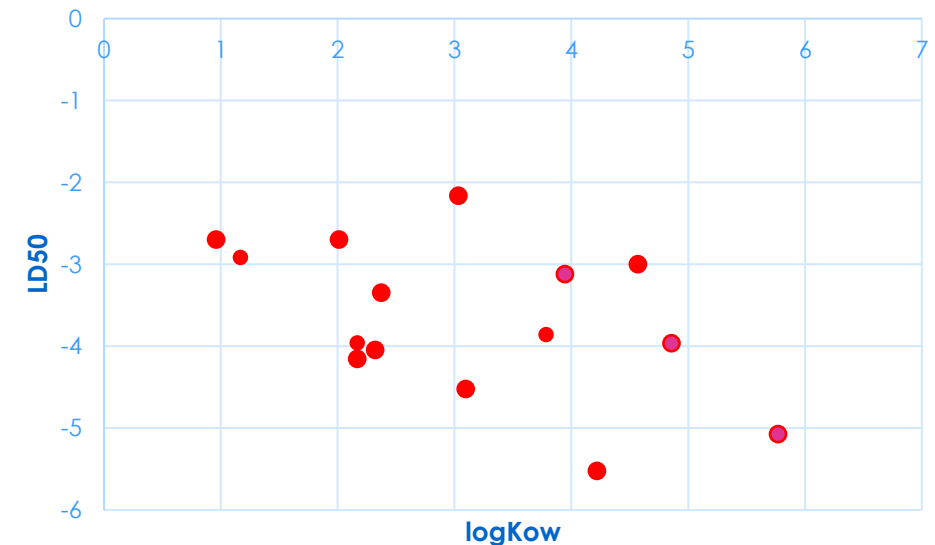
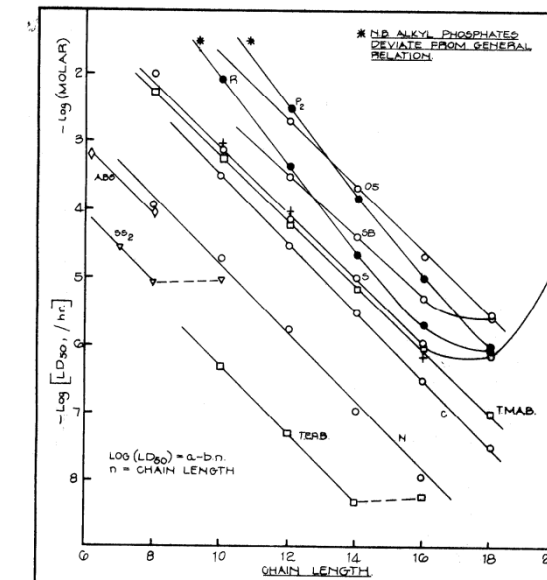
Gredelj et al. Environ. Sci.: Processes Impacts 2025

Literature Experimental Studies

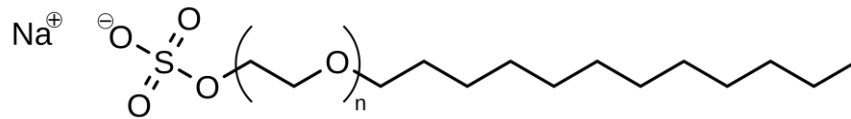


Experiments looking a HeLa cells show increasing toxicity with increasing chain length for several different headgroups

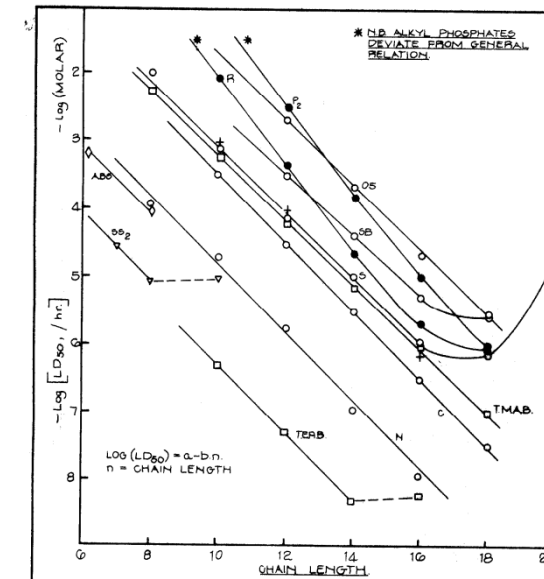
Traditional logKow method fails to yield an overall Trend for fixed chain-length (12 Carbons)



Literature Experimental Studies



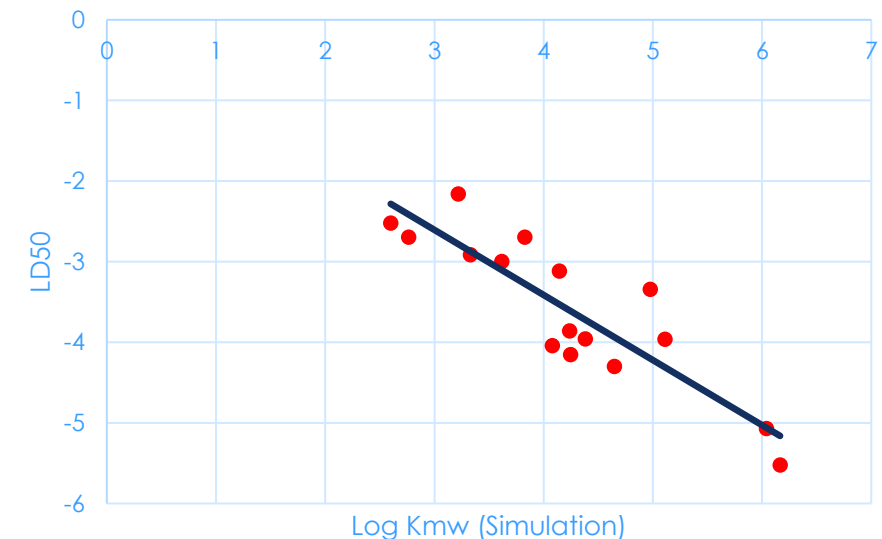
Experiments looking at HeLa cells show increasing toxicity with increasing chain length for several different headgroups



Traditional $\log K_{ow}$ method fails to yield an overall Trend for fixed chain-length (12 Carbons)

Membrane water simulations cause overall curve collapse

Conclusion : Membrane partitioning predicted from simulation predicts surfactant toxicity in vitro



Skin Penetration

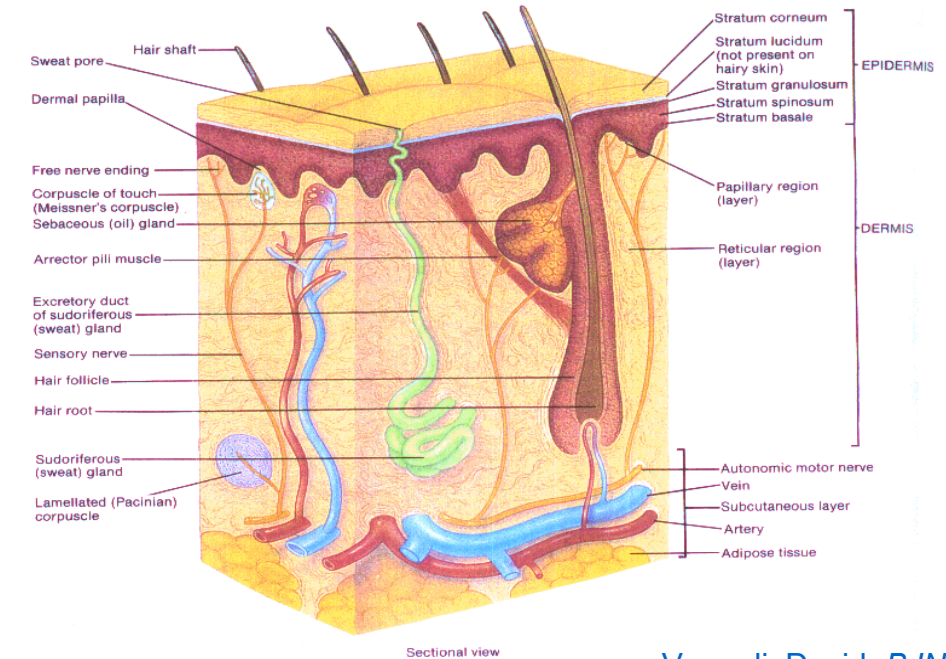


Skin Penetration

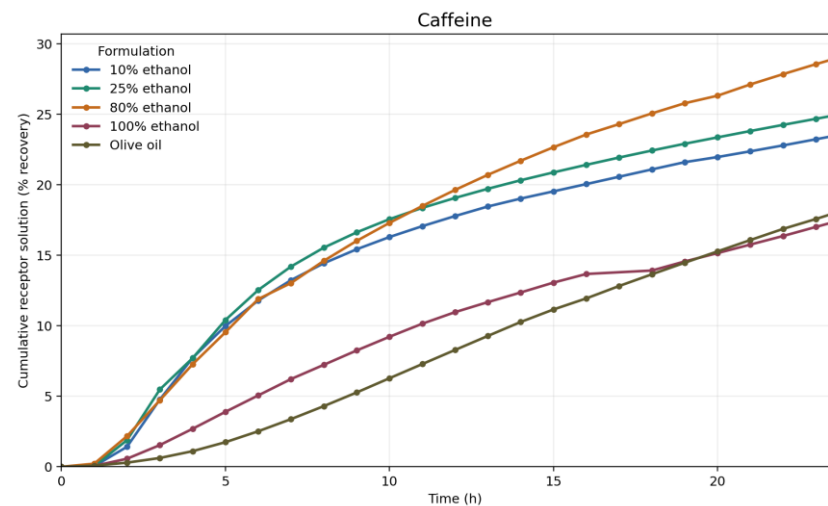
Skin is a complex structure of proteins, lipids with pores, blood vessels and other intricacies which all affect the penetration of different chemicals .

Typical method on real human skin with radiolabelled chemicals is expensive.

Both **chemical** and **formulation** properties affects skin penetration



Voegeli, David. *BJN* (2011)



Skin Penetration

Surrogate membranes

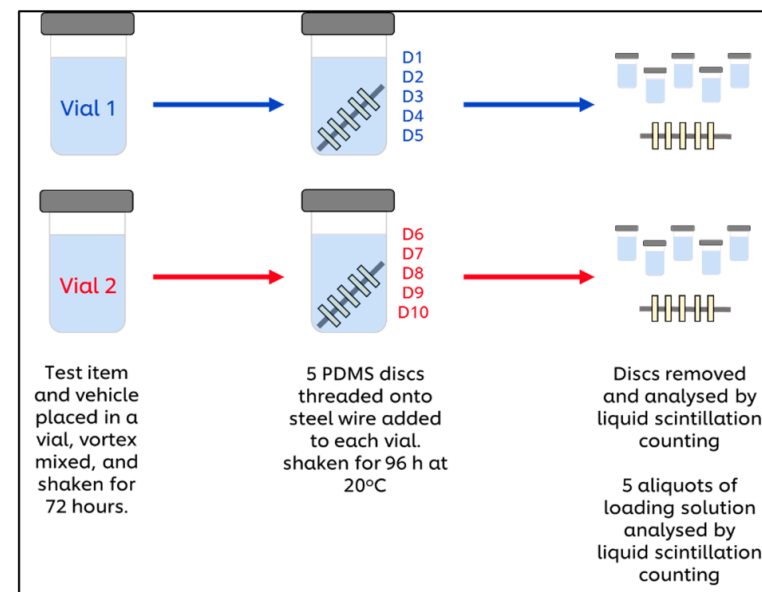
Assume that initial partitioning into skin is formulation dependent but diffusion remains constant

$$K_{i,j} \sim e^{\beta E_i} / e^{\beta E_j}$$

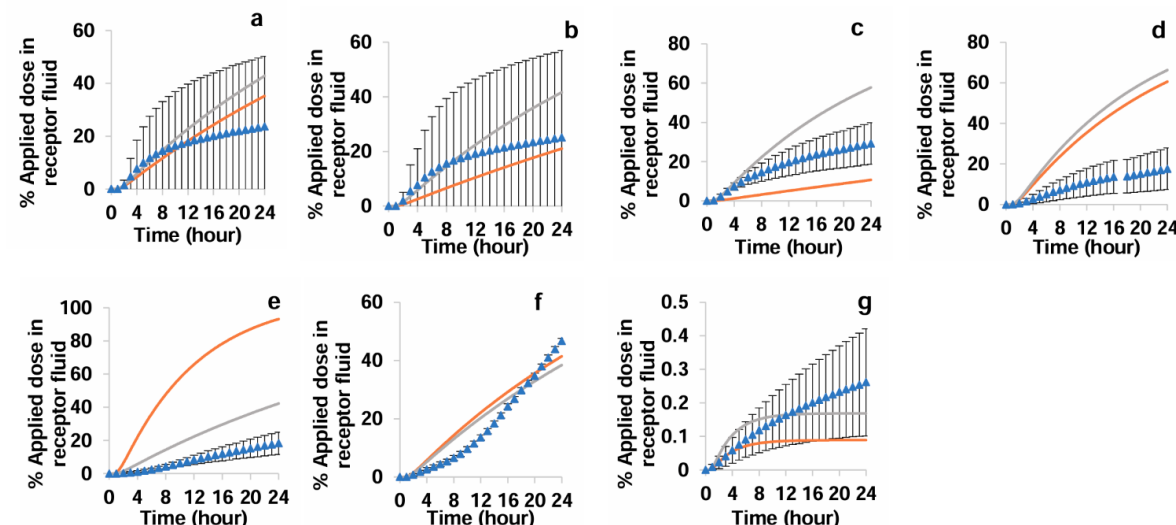
Assume Stratum Corneum similar to hydrophobic polymer PDMS

Use water as reference formulation

$$K_{SC,v} = \frac{K_{SC,w}}{K_{w,v}} = K_{SC,w} \frac{K_{v,PDMS}}{K_{w,PDMS}}$$



Caffeine



Skin Penetration

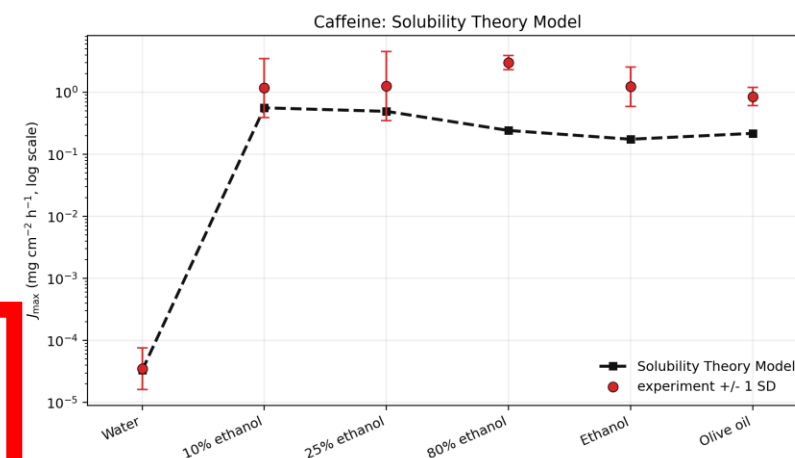
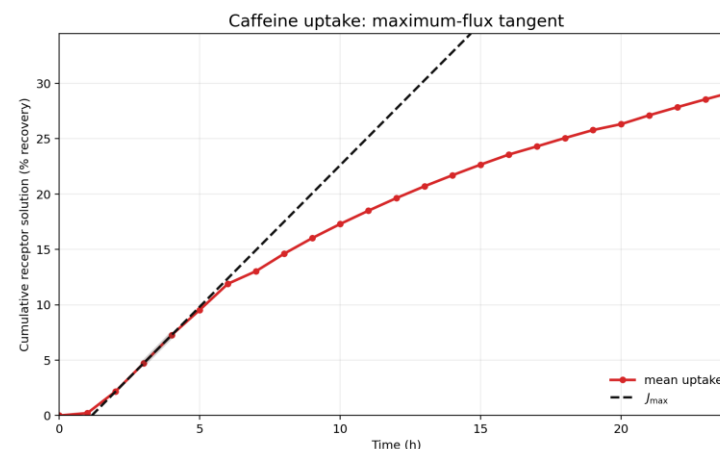
Solubility Theory

Reduce uptake curves to just early maximum flux J_{max}

Hansen Solubility Parameters characterise solubility of compounds in terms of δD (Dispersion), δP (Polarity) & δH (Hydrogen bonding)

Combined with solubility theory we can approximately predict the formulation effects

Conclusion : Skin partitioning physics can gain Insights from both polymer and solution theory in future



$$J_i = J_0 \frac{a_i}{1 + a_i} \exp(\lambda_v V_i^{2/3})$$

$$a_i = a_0 x_i \exp(-b \Delta G_i / RT)$$

$$x_i = C_i / MW_i$$

$$\Delta G_i = \Delta G_{i,sc} - \Delta G_{i,v} - \Delta \tilde{G}_{v,sc}$$

$$\Delta G_{i,sc} = V_i R a_i^2$$

$$\Delta G_{i,v} = \sum_{k \in v} w_k V_i R a_{i,k}^2$$

$$\Delta \tilde{G}_{v,sc} = V_v R a_{v,sc}^2 - \langle V_v R a_{v,sc}^2 \rangle$$

$$R a_{i,j}^2 = 4(\delta D_i - \delta D_j)^2 + (\delta P_i - \delta P_j)^2 + (\delta H_i - \delta H_j)^2$$

Skin Penetration

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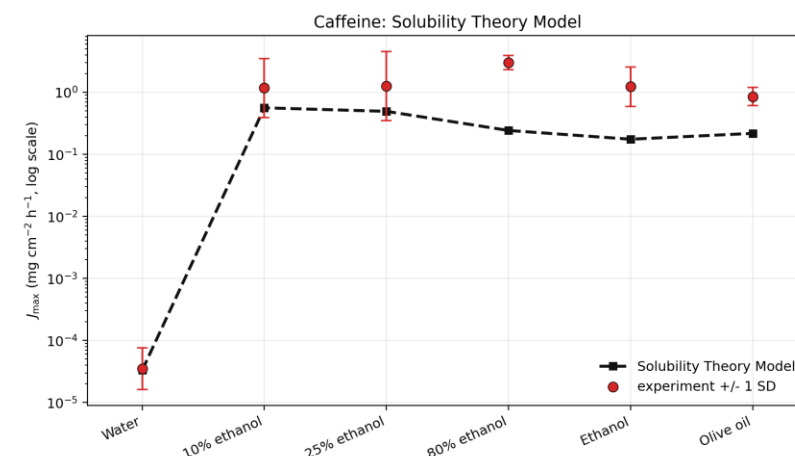
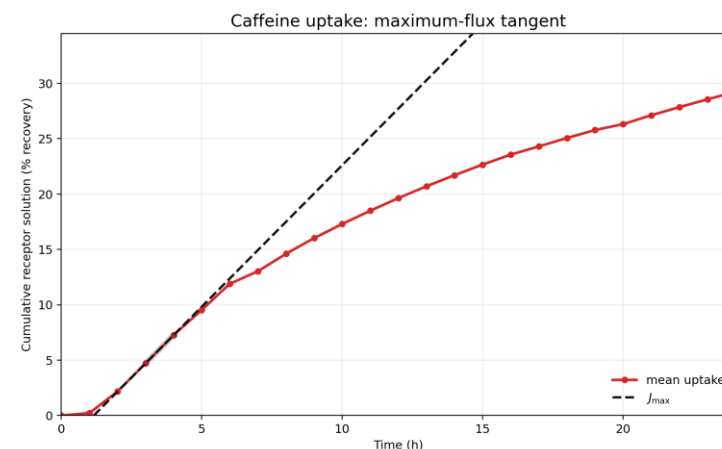
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$$\Delta G_i = \Delta G_{i,sc} - \Delta G_{i,v} - \Delta \tilde{G}_{v,sc} \quad R a_{i,j}^2 = 4(\delta D_i - \delta D_j)^2 + (\delta P_i - \delta P_j)^2 + (\delta H_i - \delta H_j)^2$$



Conclusion : Skin partitioning physics can gain Insights from both polymer and solution theory in future

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Overall Conclusion

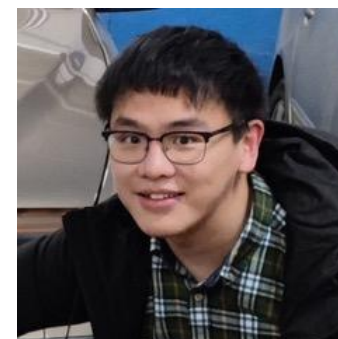
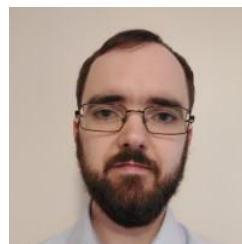
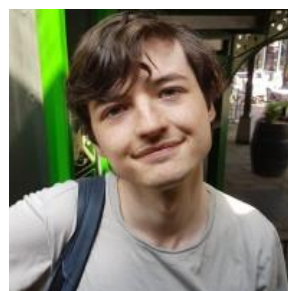
Soft matter science offers many opportunities for developing alternatives to animal testing

- Lung Surfactant Inhibition
- Surfactant Toxicity
- Skin Absorption

Acknowledgements



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Thank you and Questions?